



Bayesian data assimilation for cardiovascular flow using bi- fidelity Ensemble Kalman Inversion

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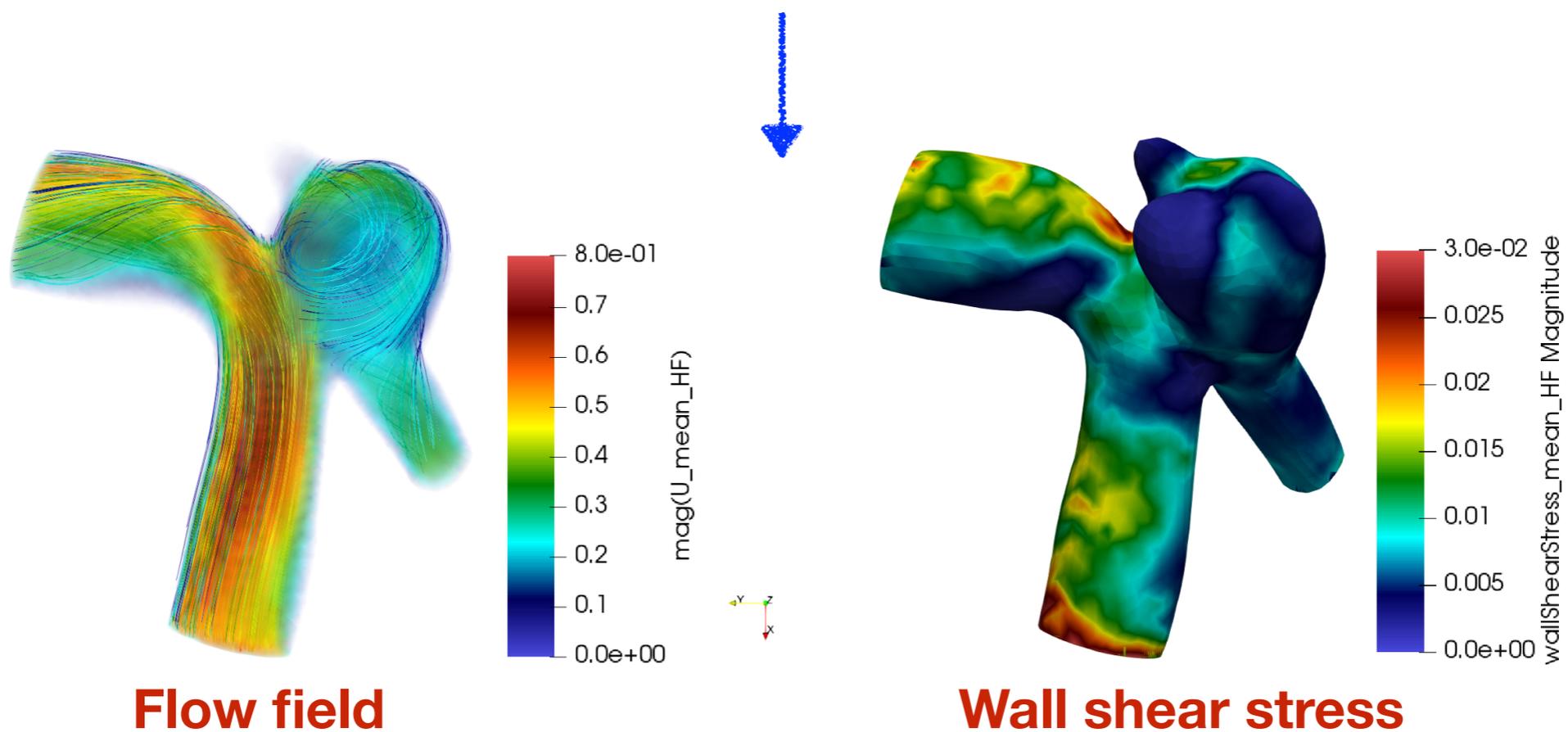
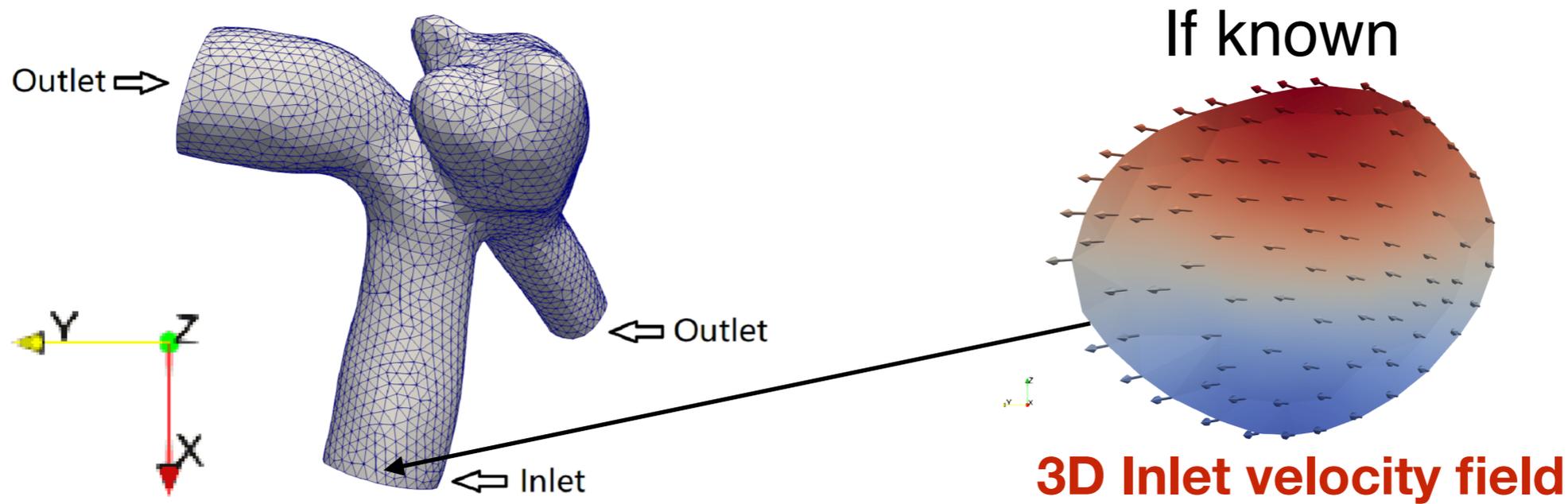
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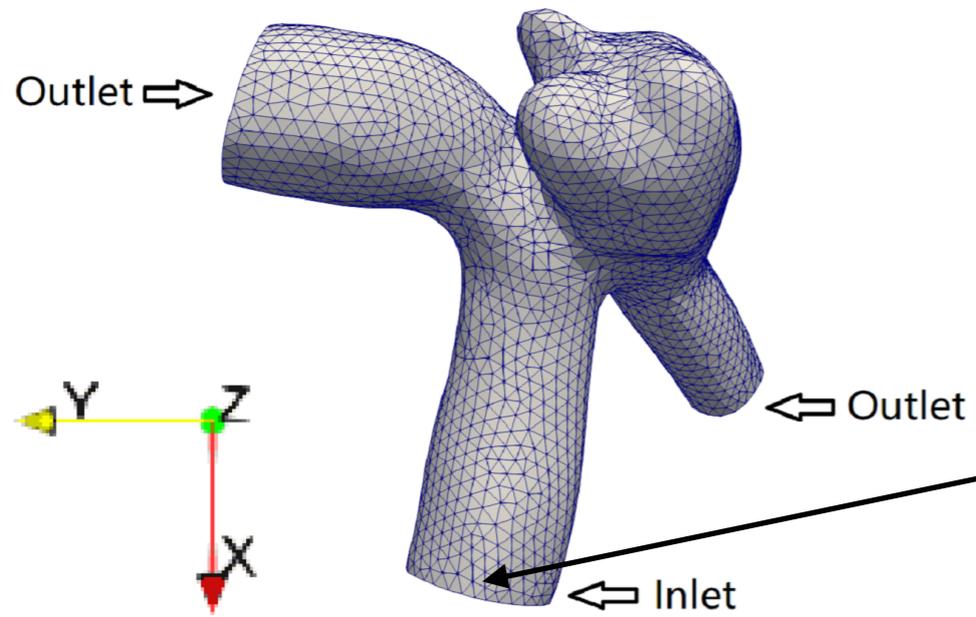
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Example: Inlet inversion in aneurysm bifurcation



Example: Inlet inversion in aneurysm bifurcation



Not known



3D Inlet velocity field

Infer



Sparse, noisy flow measurements

Example: Inlet inversion in aneurysm bifurcation

Not known



θ

$F(\theta)$
CFD model

y



3D Inlet velocity field

Sparse, noisy flow
measurements (Data)

$$\hat{x} = F(\theta, x_0) = \tilde{x} + \sigma_m$$

$$y = H(\tilde{x}) + \sigma_d$$

Assimilate sparse data into model

$$P(\hat{x}, \theta | y) \sim P(\theta)P(y | \theta)$$

Bayes rule

Assumptions

Linear forward

$$\hat{x}_t = F(x_{t-1}) + \sigma_m$$

Gaussian
Prior

$$y_t = H\tilde{x}_t + \sigma_d$$

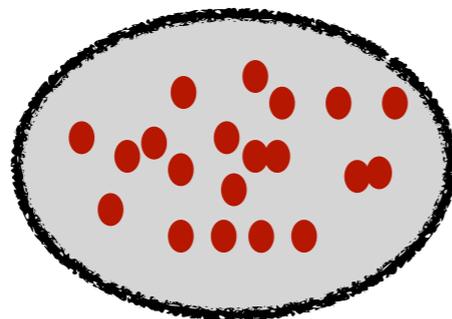
Gaussian
Likelihood

Posterior

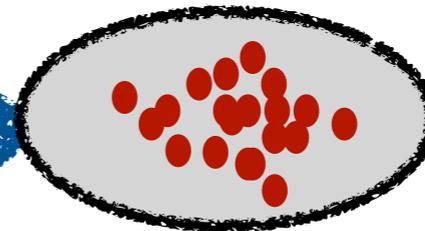
$$x_t^{(j)} = \hat{x}_t^{(j)} + C_{\hat{x}_t \hat{x}_t} H^T (H C_{\hat{x}_t \hat{x}_t} H^T + \Gamma)^{-1} (y_t^{(j)} - H \hat{x}_t^{(j)})$$

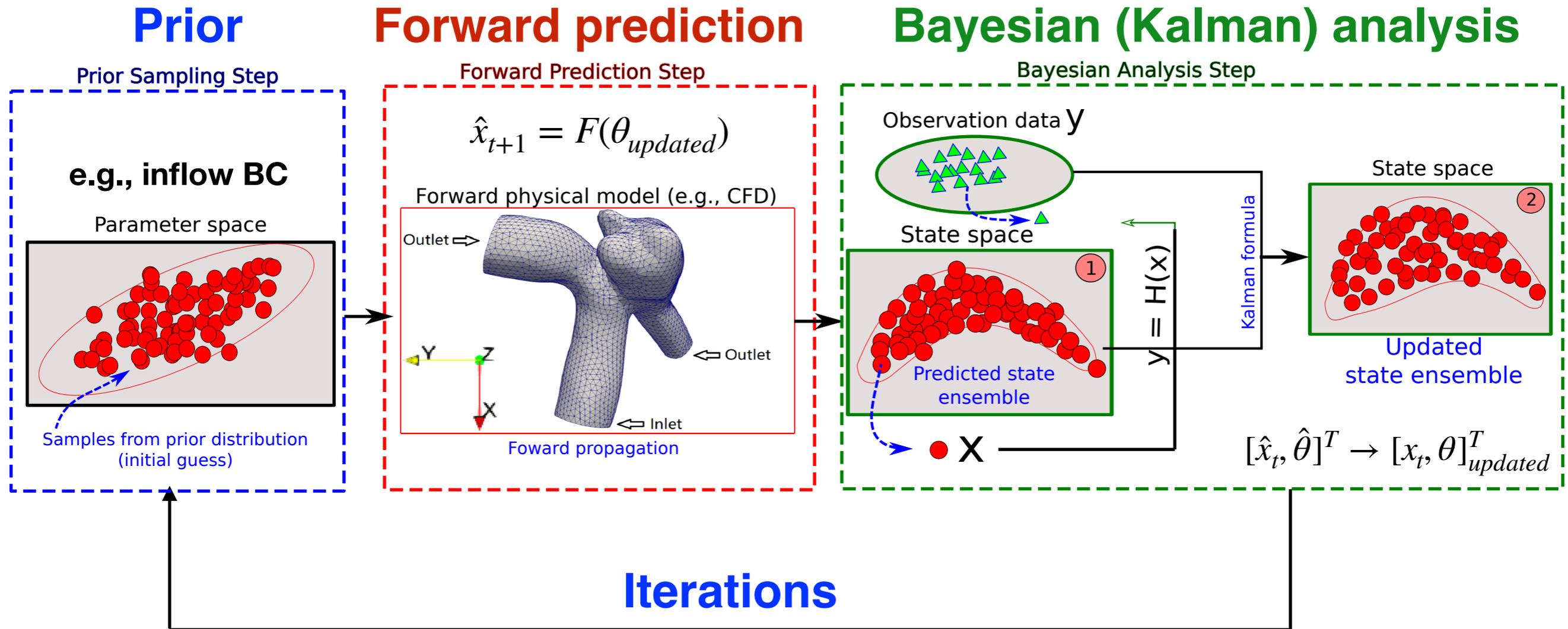
Kalman update formula for state estimation

Prior ensemble



Posterior ensemble





Proposed by M. Iglesias, A. Stuart, 2013, 2017, 2018

This is also can be roughly formulated as a constrained optimization problem

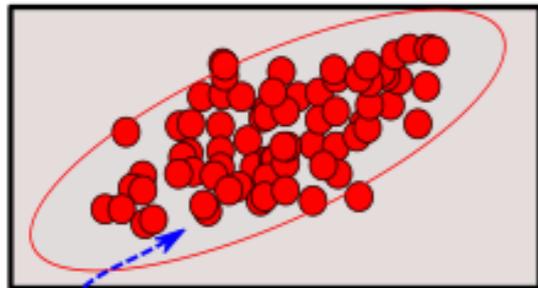
$$\min_{\theta, x} \|\bar{y} - Hx\|^2, \quad s.t. \quad x = F(\theta)$$

Prior

Prior Sampling Step

e.g., inflow BC

Parameter space

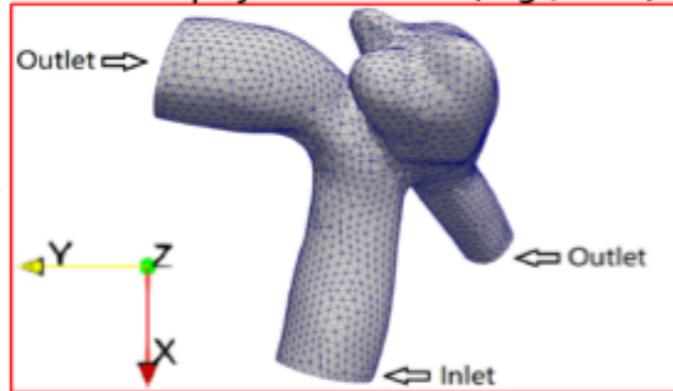


Forward prediction

Forward Prediction Step

$$\hat{x}_{t+1} = F(\theta_{updated})$$

Forward physical model (e.g., CFD)



Forward propagation

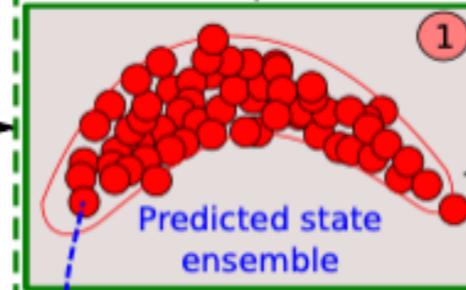
Bayesian (Kalman) analysis

Bayesian Analysis Step

Observation data y



State space

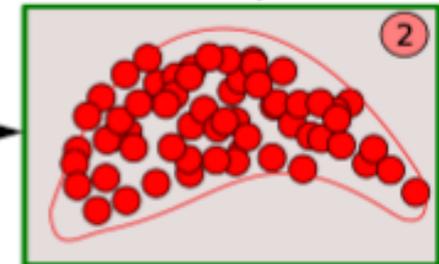


X

$$y = H(x)$$

Kalman formula

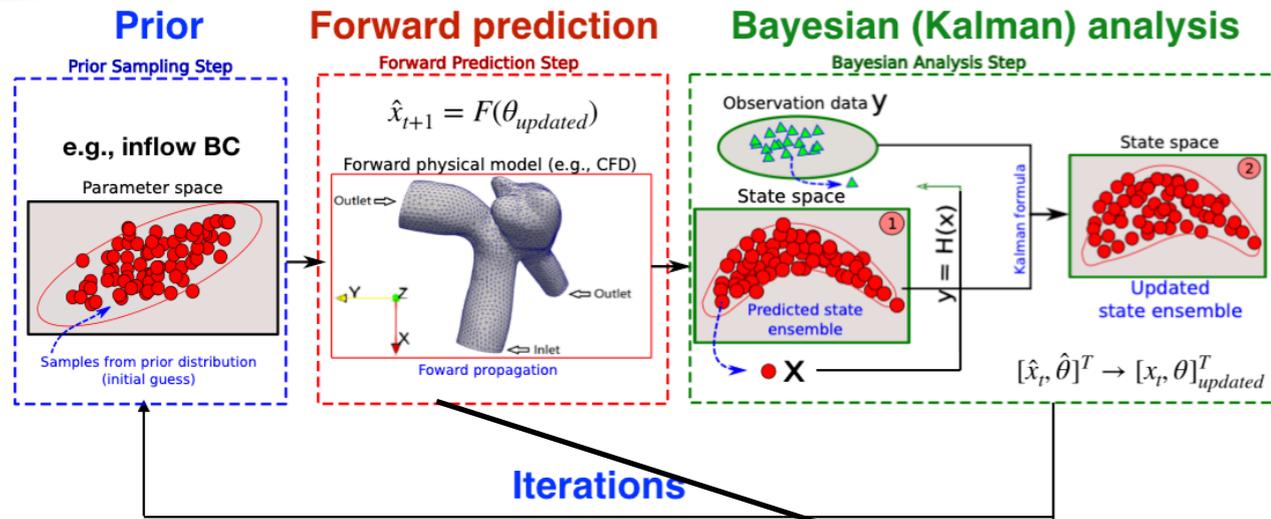
State space



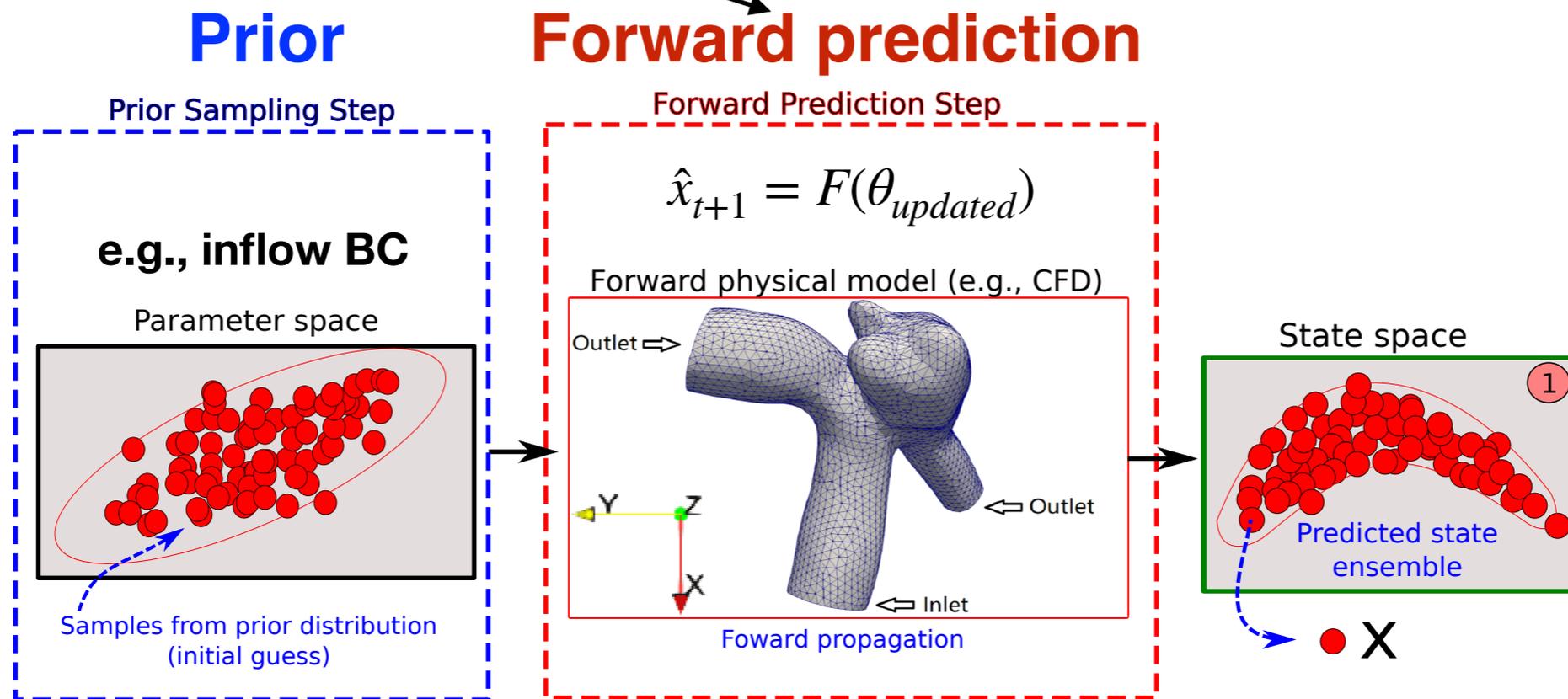
Updated state ensemble

$$[\hat{x}_t, \hat{\theta}]^T \rightarrow [x_t, \theta]_{updated}^T$$

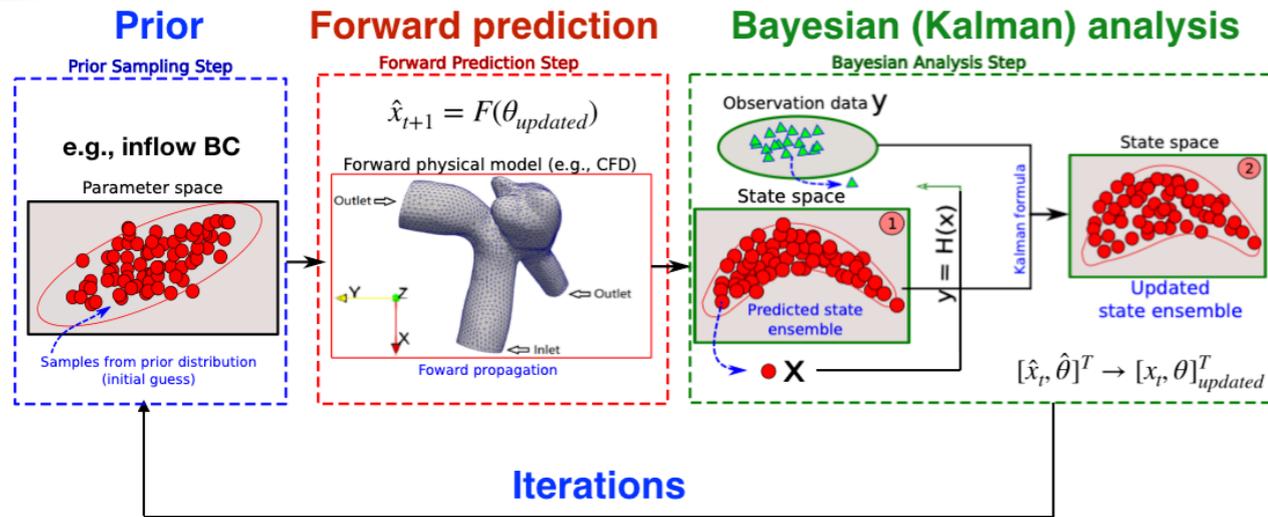
Iterations



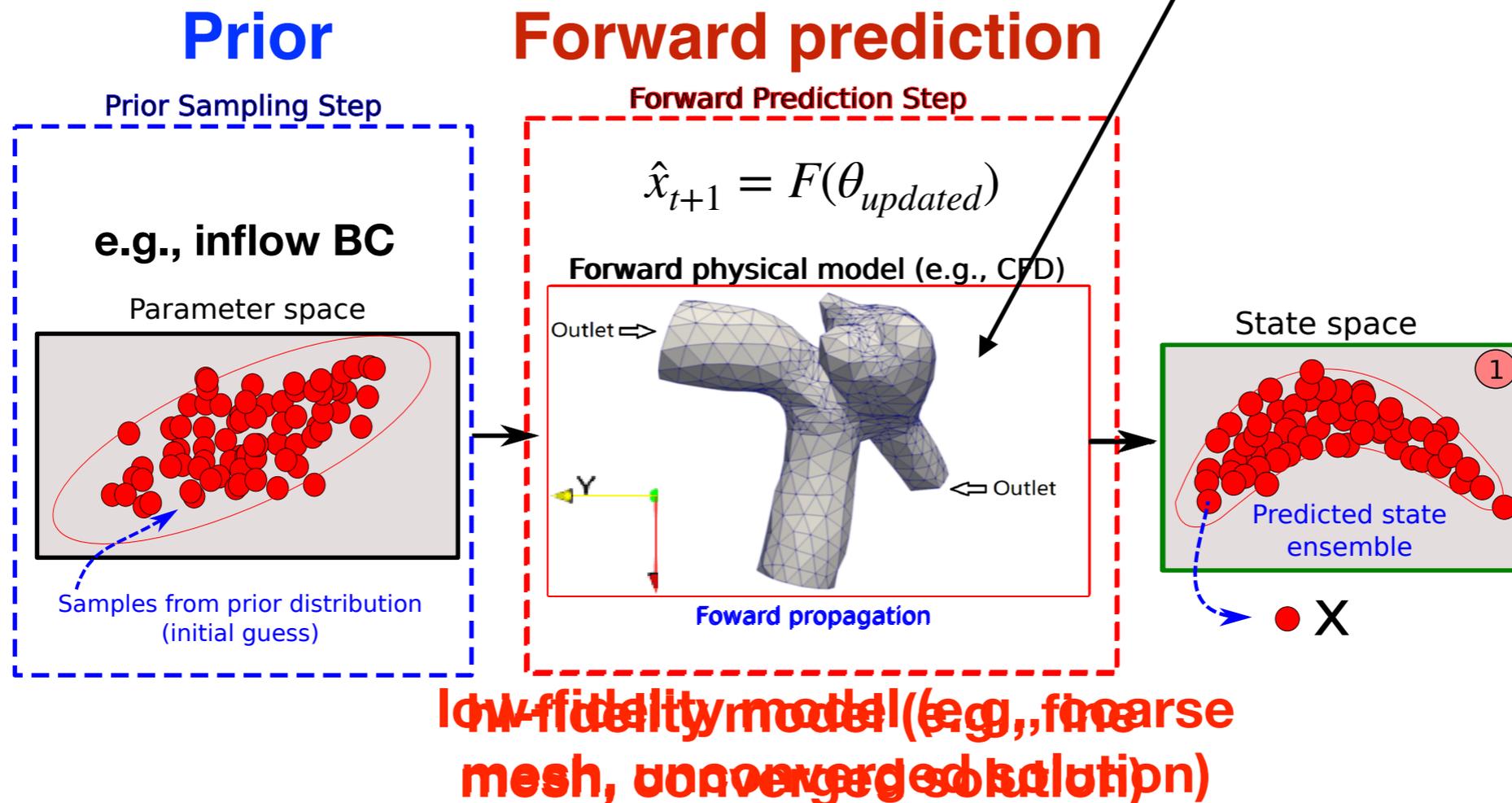
How to reduce the computational cost?



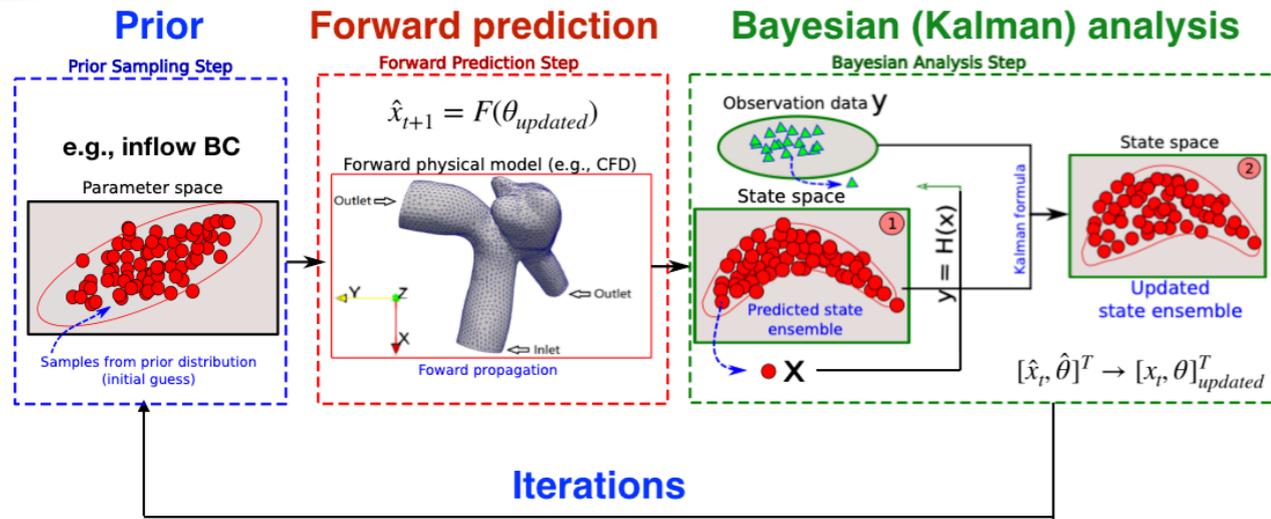
**Many evaluations of forward model, so if forward evaluation is expensive
of iteration * # of samples \rightarrow Computationally prohibitive!**



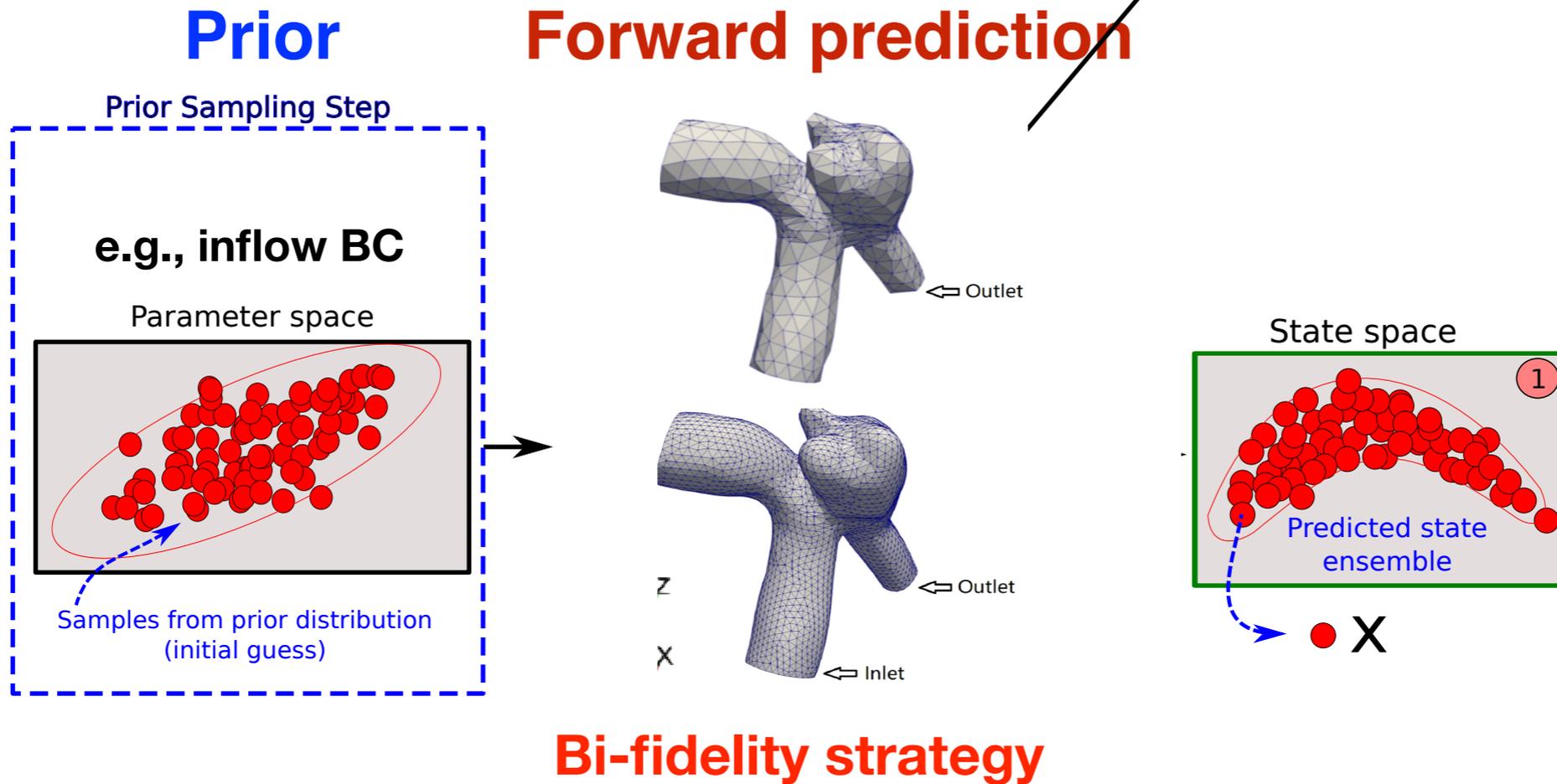
Replace the hi-fidelity forward model with the low-fidelity model



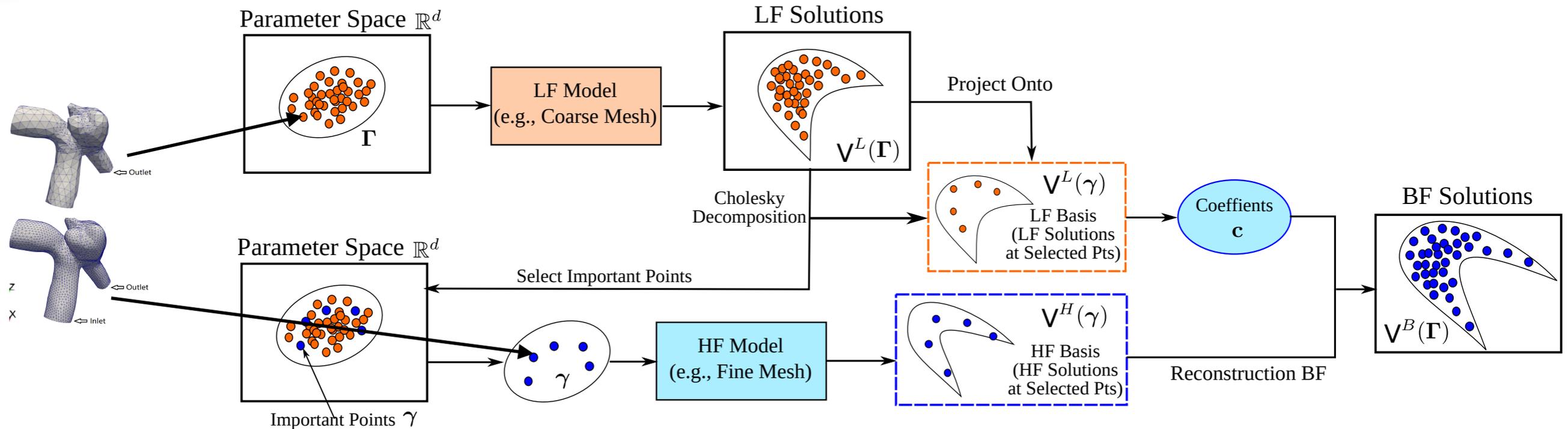
However, low-fidelity model predictions has low accuracy, and thus inferred results could be very wrong!



Leverage the accuracy of high-fidelity model and efficiency of low-fidelity model



Proposed bi-fidelity iterative ensemble Kalman inversion approach



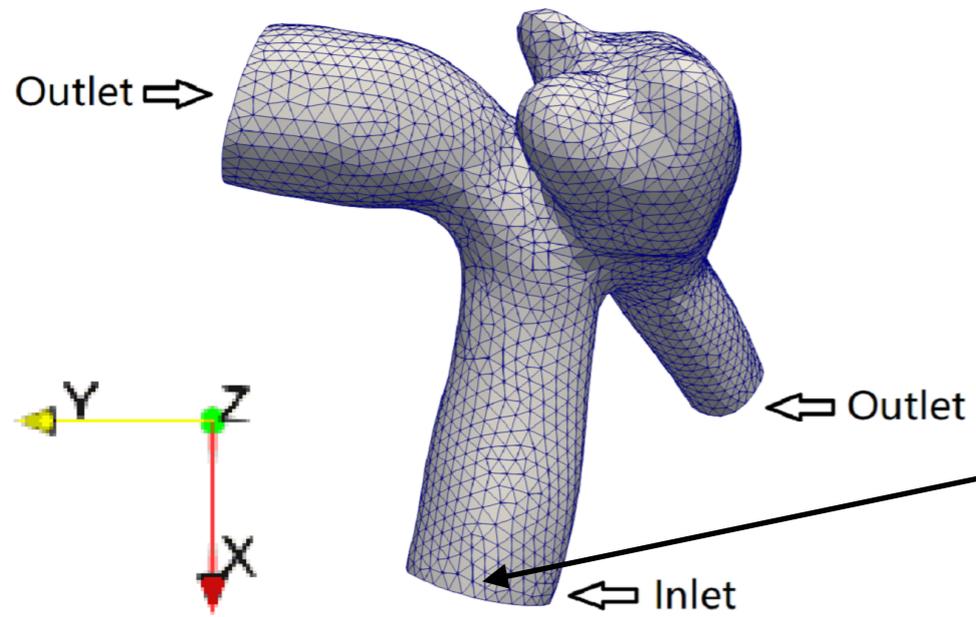
Empirical error estimation for BF solver

Theorem 1. Given the first $k + 1$ pre-selected important points γ^{k+1} , the relative error between the bi-fidelity solution and the high-fidelity solution can be bounded for any point $\mathbf{z}_* \in \Gamma$ as follows:

$$\begin{aligned}
 \frac{\|\mathbf{v}^H(\mathbf{z}_*) - \mathbf{v}^B(\mathbf{z}_*)\|}{\|\mathbf{v}^H(\mathbf{z}_*)\|} &\leq \underbrace{\frac{d^H(\mathbf{v}^H(\mathbf{z}_*), \mathbb{U}^H(\gamma^k))}{\|\mathbf{v}^H(\mathbf{z}_*)\|}}_{\text{relative distance}} + \underbrace{\frac{\|P_{\mathbb{U}^H(\gamma^k)} \mathbf{v}^H(\mathbf{z}_*) - \mathbf{v}^B(\mathbf{z}_*)\|}{\|\mathbf{v}^H(\mathbf{z}_*)\|}}_{\text{in-plane error}} \\
 &= \frac{d^H(\mathbf{v}^H(\mathbf{z}_*), \mathbb{U}^H(\gamma^k))}{\|\mathbf{v}^H(\mathbf{z}_*)\|} \left(1 + \frac{\|P_{\mathbb{U}^H(\gamma^k)} \mathbf{v}^H(\mathbf{z}_*) - \mathbf{v}^B(\mathbf{z}_*)\|}{\frac{d^H(\mathbf{v}^H(\mathbf{z}_*), \mathbb{U}^H(\gamma^k))}{\|\mathbf{v}^H(\mathbf{z}_*)\|}} \right),
 \end{aligned} \tag{11}$$



Test Case: Inlet inversion in aneurysm bifurcation



Not known

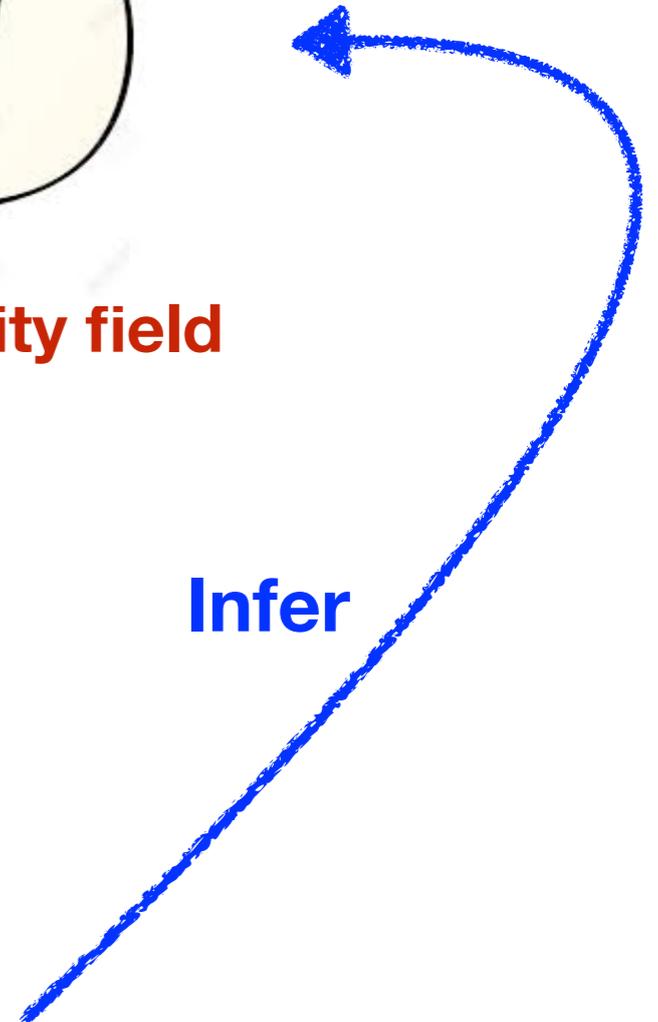


3D Inlet velocity field

Infer



Sparse, noisy flow measurements

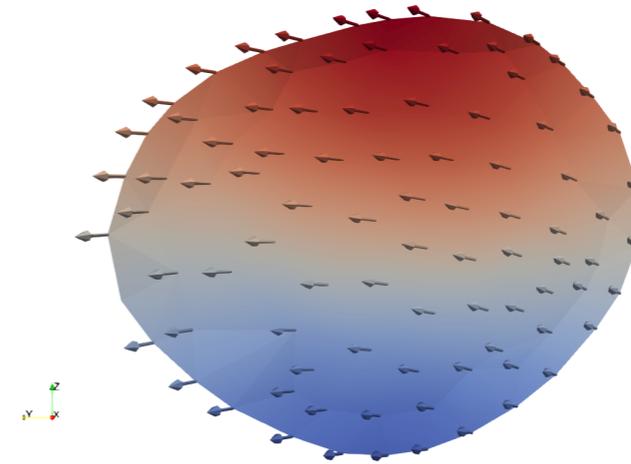


Test Case: Inlet inversion in aneurysm bifurcation



Generate synthetic data

Sample out 0.4% flow data, corrupted with 40% noise



Inlet ground truth (Not known)

Prior distribution of inlet

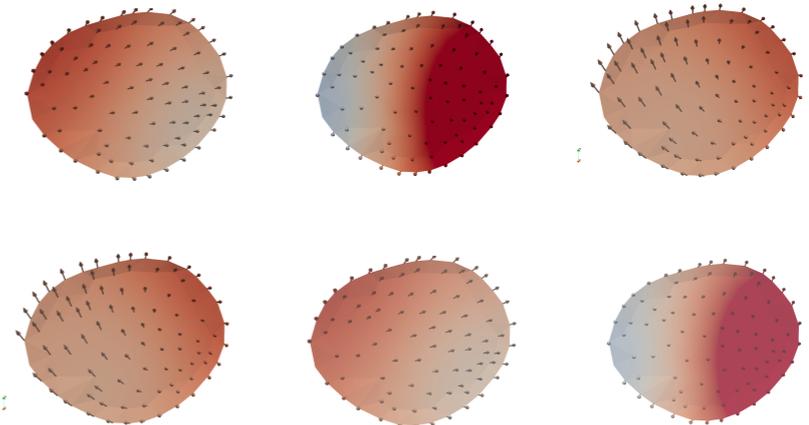
Gaussian process

$$f(\mathbf{x}) \sim \mathcal{GP}(0, K(\mathbf{x}, \mathbf{x}')), \quad K(\mathbf{x}, \mathbf{x}') = \sigma_0^2 \exp\left(-\frac{|\mathbf{x} - \mathbf{x}'|}{2l^2}\right)$$

$$f(\mathbf{x}) = \sum_{i=1}^{n_k \rightarrow \infty} \sqrt{\lambda_i} \phi_i(\mathbf{x}) \omega_i$$

$$\mathbf{u}_{in} = \mathbf{u}_{in}^{base} + [f_x(\mathbf{x}), f_y(\mathbf{x}), f_z(\mathbf{x})]$$

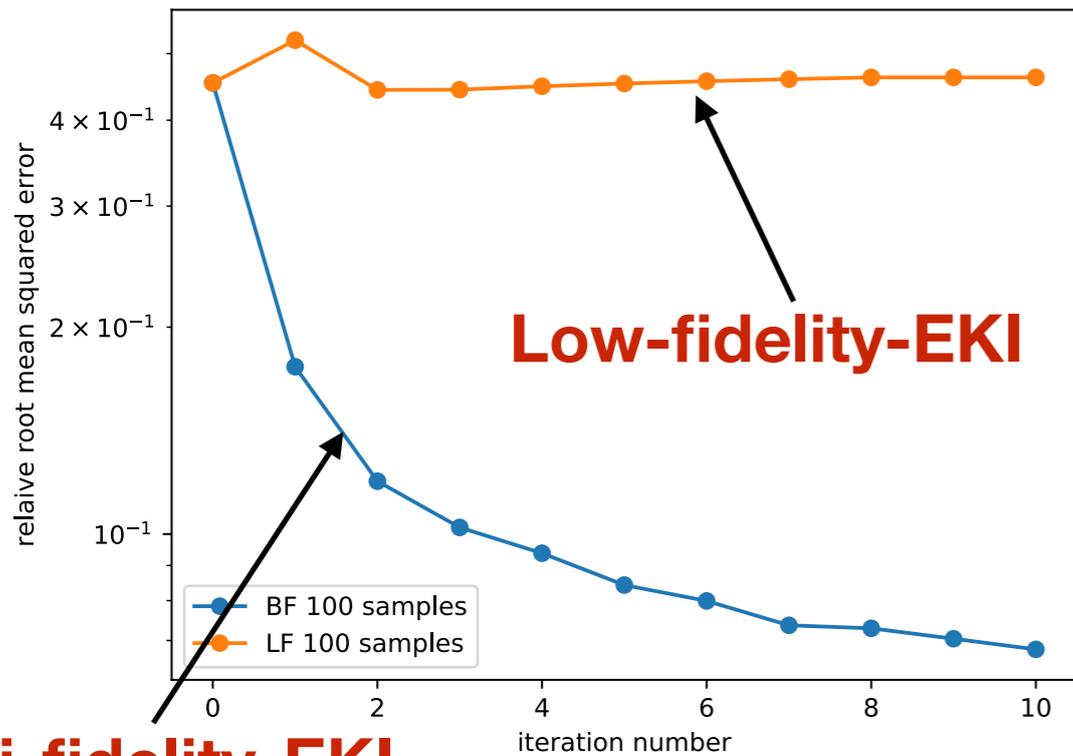
Some prior samples



9-dimensional inverse problem



Convergence history



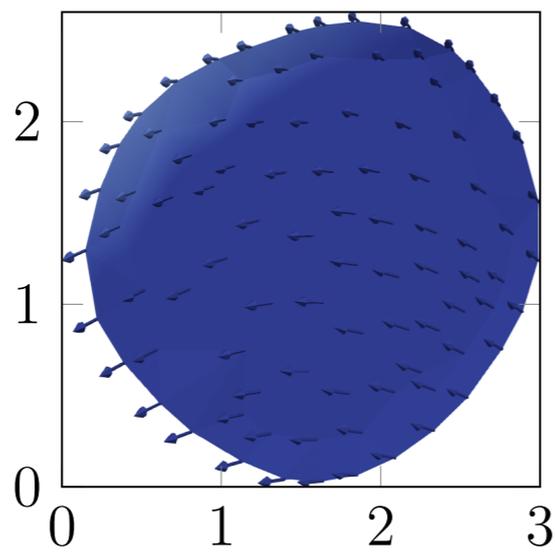
100 Samples for each iteration for 10 iterations

Hi-fidelity-EKI: 30 hours

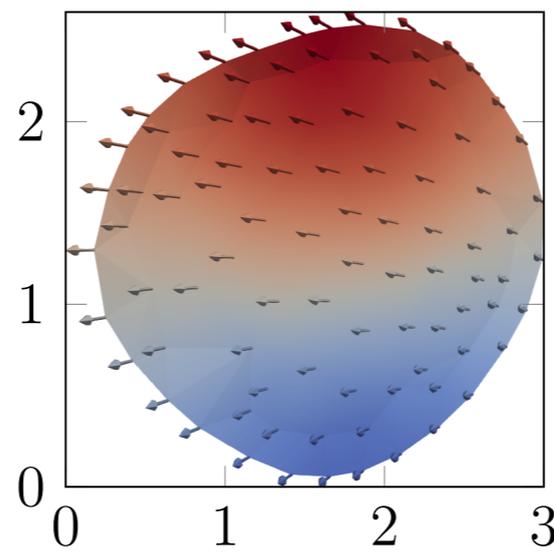
Bi-fidelity-EKI: 0.15 hours (9 mins)!

More than 200 times speedup!

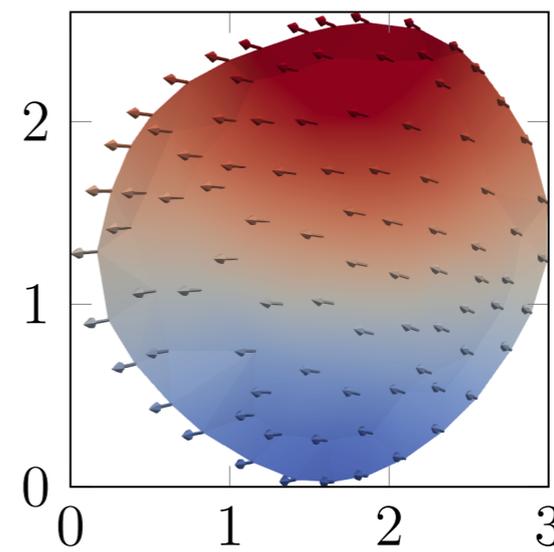
Bi-fidelity-EKI



LF-EKI-Inferred



BF-EKI-Inferred



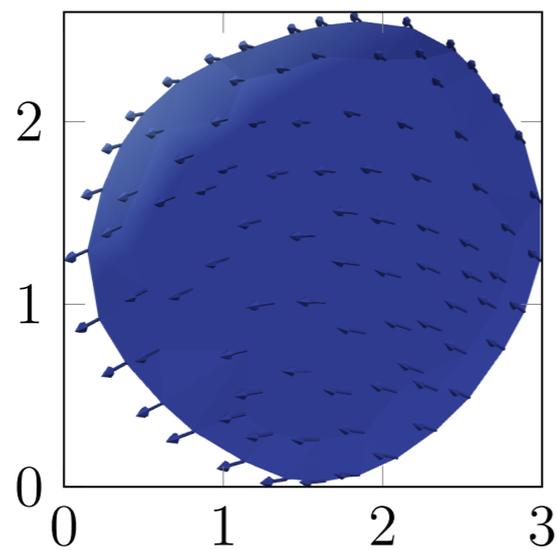
Ground truth



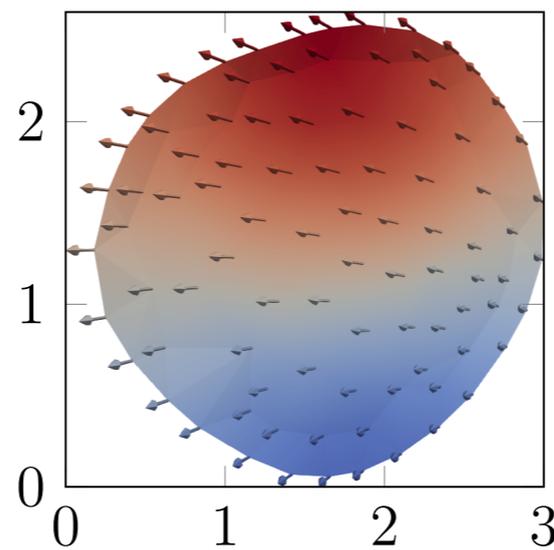
How do we quantify the uncertainty?



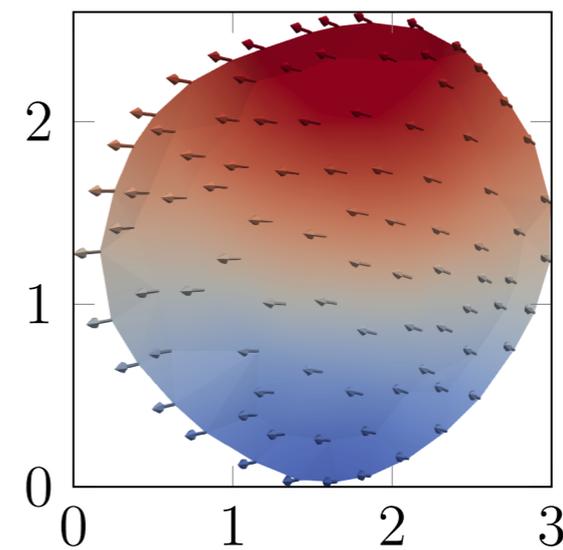
We need to use fully Bayesian method to quantify the uncertainty!



LF-EKI-Inferred



BF-EKI-Inferred



Ground truth



Fully Bayesian or MCMC methods are computationally expensive; however, in order to validate our method, we did a proof-of-concept case to illustrate how it works:

1. Simplify the case to an 2D steady simulation of aorta dissection and infer inlet velocity magnitude from observation data from 4D flow MRA

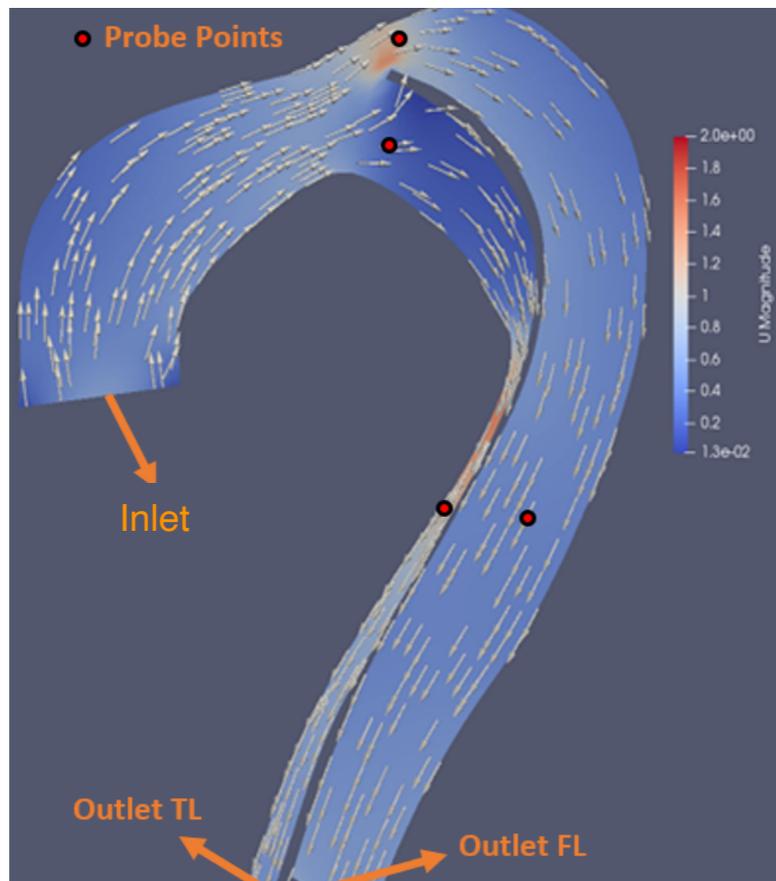
2. From EKI, we obtained an accurate mean $U=0.6$. Then we assign a prior within interval $(0,1)$ and perform MCMC.

$$P(\theta) = \text{Beta}(1.1,1.1)$$

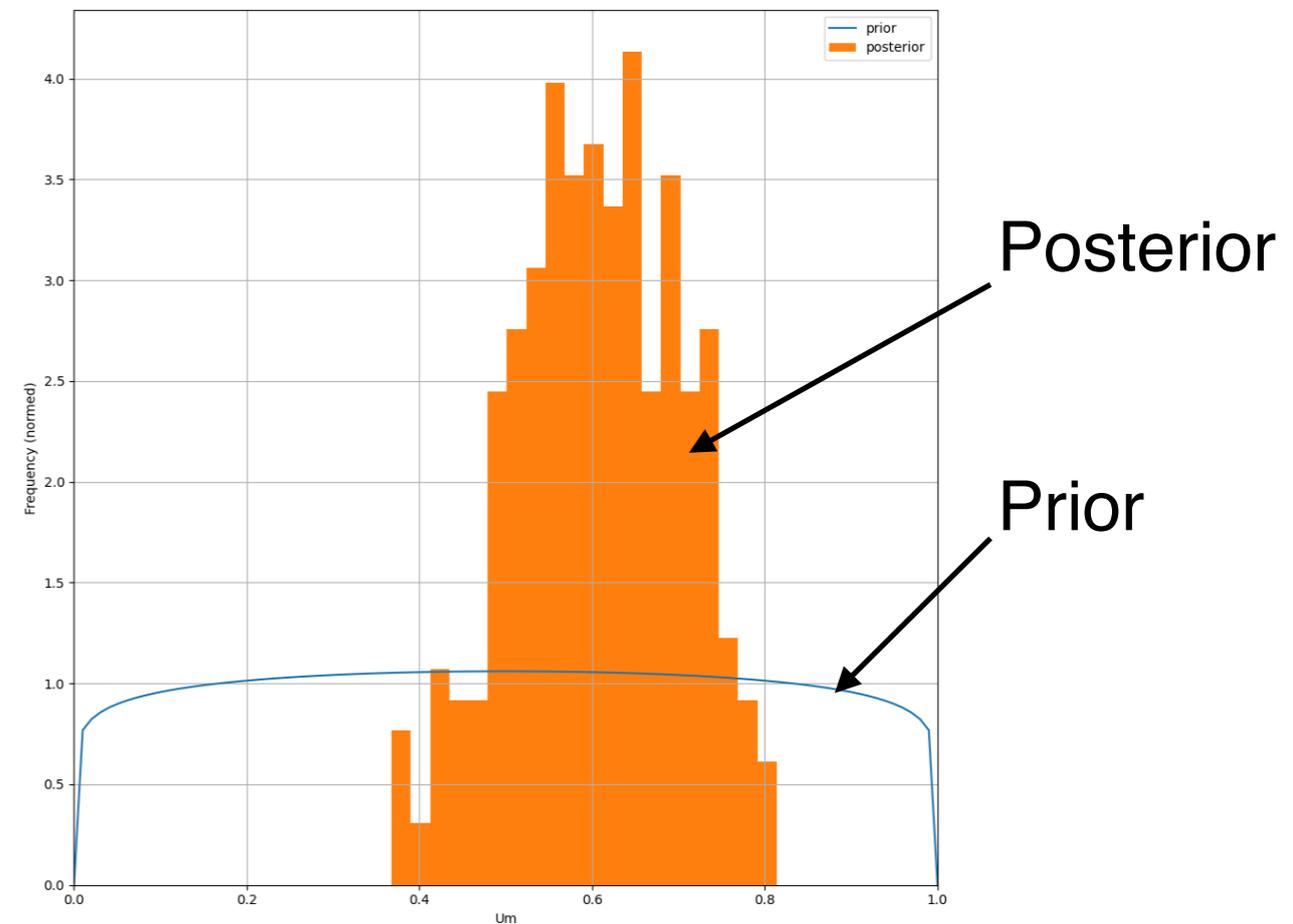
3. With the information from 4D flow MRA on the probing points distributed downstream of the aorta, the final posterior is inferred. Thus, inlet profile is predicted.

Test Case: Inlet inversion in aorta dissection

**2D steady simulation cost 1.5
seconds per case**



Probes on a 2D aorta flow field



Prior vs. Posterior

The MCMC method successfully give the uncertainty of the velocity.



Conclusion

1. We proposed a Bi-fidelity EKI method and applied it on aneurysm bifurcation inversion problem. The method leverages the accuracy of hi-fidelity model and efficiency of low-fidelity model and yields accurate mean inlet velocity profile with economical computational cost.
2. Besides predicting mean accurately, we have to quantify uncertainty. We adopted MCMC to quantify the velocity magnitude. A aorta dissection case is used for validation and the proposed method gives accurate uncertainty.
3. Future work will apply EKI and fully Bayesian method on 3D simulations to predict mean and uncertainty accurately.

Related Publications

1. H. Gao, X. Zhu, J.-X. Wang. “**A Bi-fidelity Surrogate Modeling Approach for Uncertainty Propagation in Three-Dimensional Hemodynamic Simulations**”. *CMAME*, 2019. (Under revision)[[Arxiv](#)]
2. H. Gao, J.-X. Wang. “**A Bi-fidelity Ensemble Kalman Inversion Approach for Inverse Problems in Fluid Simulations**”. 2019. (In preparation)
3. J. Wu, J.-X. Wang, S. C. Shadden, “**Improving the Convergence of the Iterative Ensemble Kalman Filter by Resampling**”, 2019. [[Arxiv](#)]
4. J. Wu, J.-X. Wang, S. C. Shadden, “**Adding constraints to Bayesian inverse problems**”, [2019 AAAI Conference on Artificial Intelligence](#), 2019



Thank you!

